

Research



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# Singers show enhanced performance and neural representation of vocal imitation

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Humans have a remarkable capacity to finely control the muscles of the larynx, via distinct patterns of cortical topography and innervation that may underpin our sophisticated vocal capabilities compared with non-human primates. Here, we investigated the behavioural and neural correlates of laryngeal control, and their relationship to vocal expertise, using an imitation task that required adjustments of larynx musculature during speech. Highly trained human singers and non-singer control participants modulated voice pitch and vocal tract length (VTL) to mimic auditory speech targets, while undergoing real-time anatomical scans of the vocal tract and functional scans of brain activity. Multivariate analyses of speech acoustics, larynx movements and brain activation data were used to quantify vocal modulation behaviour and to search for neural representations of the two modulated vocal parameters during the preparation and execution of speech. We found that singers showed more accurate task-relevant modulations of speech pitch and VTL (i.e. larynx height, as measured with vocal tract MRI) during speech imitation; this was accompanied by stronger representation of VTL within a region of the right somatosensory cortex. Our findings suggest a common neural basis for enhanced vocal control in speech and song.

This article is part of the theme issue ‘Voice modulation: from origin and mechanism to social impact (Part I)’.

## 1. Introduction

Many cognitive, neural and physiological adaptations have been implicated in the evolution of human speech [1–3]. When comparing our species with the other great apes, one major distinction concerns the neural control of the larynx (or voice box). In humans, anatomical studies have revealed that the larynx receives innervation via direct connections from the primary motor cortex to the nucleus ambiguus, while in other apes this pathway is relatively more sparse, and in monkeys it is absent [4–7]. One hypothesis proposes that this direct pathway facilitates the rapidity and precision of laryngeal control in

human speech and song, for example in the initiation of vocalization, the fine tuning of vocal pitch and voice quality and in switching between voiced and unvoiced segments of spoken words (e.g. consecutive consonants and vowels) [7–15].

Researchers investigating the evolution of vocal behaviour in humans have been interested in measuring the acoustic correlates of laryngeal control through volitional vocal modulations. Two acoustic parameters have been particularly important in this endeavour: fundamental frequency ( $F_0$ ) and formant spacing ( $\Delta F$ ).  $F_0$  relates to the rate of vibration of the vocal folds in the larynx and is perceptually experienced as vocal pitch—in humans, adult males typically have longer and thicker vocal folds than adult females, and thus generate a lower  $F_0$  during speech.  $\Delta F$  is related to the resonant properties of the vocal tract and covaries negatively with vocal tract length (VTL)—thus, adults show lower  $\Delta F$  than children (whose vocal tracts are typically shorter), and adult male voices typically have lower  $\Delta F$  than adult female voices owing to the secondary descent of the larynx during puberty in human males. Previous research on speech acoustics has shown that humans can readily modulate  $\Delta F$  in the appropriate direction when attempting to sound larger or smaller [16,17]. Similarly, adults and children will increase  $F_0$  and  $\Delta F$  to sound more feminine, and will decrease these parameters to sound more masculine [18–20]. Such studies have provided crucial insights into the acoustic correlates of laryngeal control, although it should be noted that we are not aware of any study to date that has shown that human  $\Delta F$  modulations are indeed achieved through changes in larynx height.

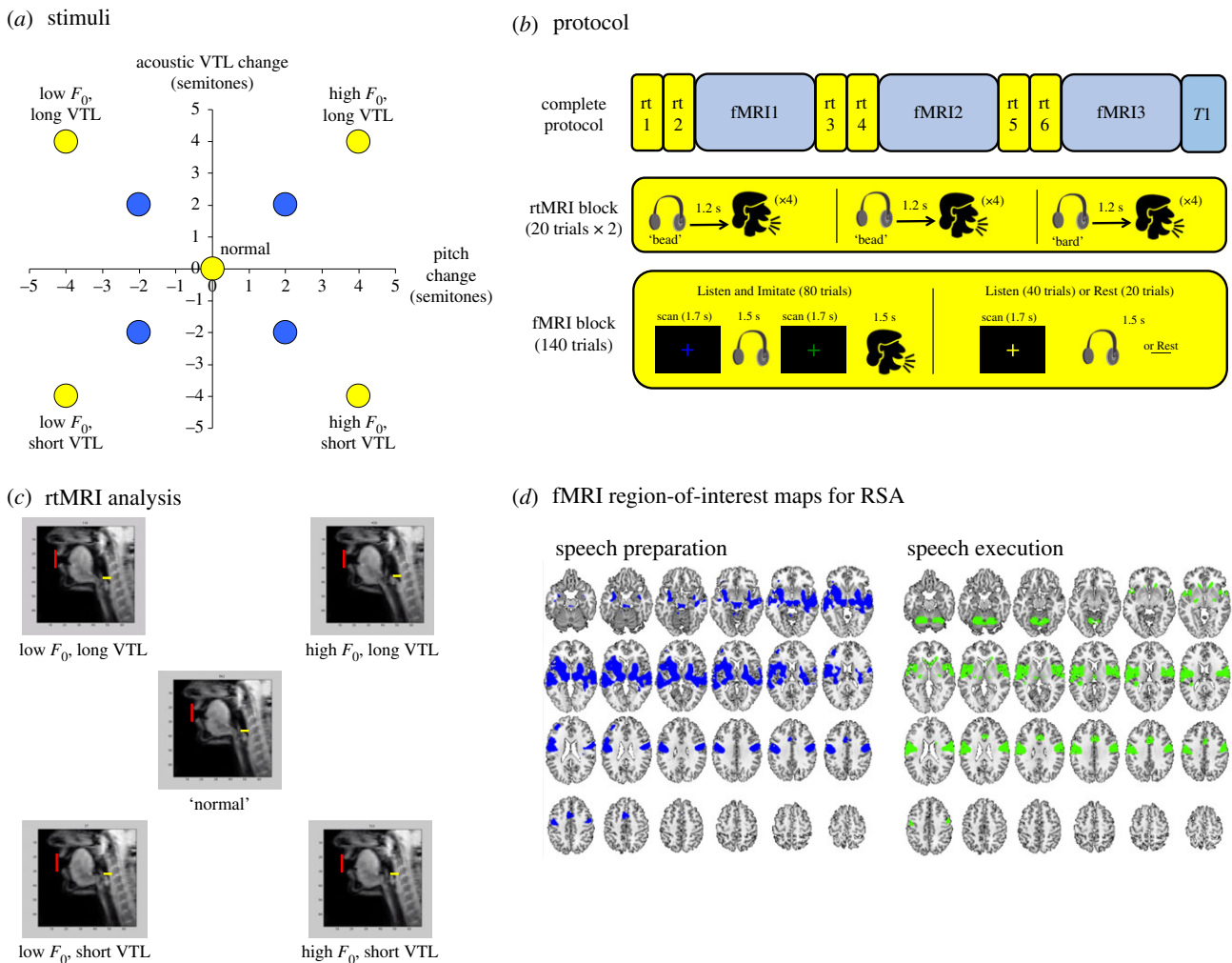
The ability to modulate the voice is potentially adaptive for individuals. For example, vocal size exaggeration is effective in changing listeners' evaluations of talker height [17], which may provide advantages in competitive situations. Furthermore, recent evidence on social trait expression has shown that talkers can volitionally modulate their speaking voice to generate exaggerated impressions of specific traits in naive listeners [21]. Beyond the mere demonstration of vocal modulation in humans, it is of interest to investigate how this skill might vary across individuals. One way to do this is to investigate expert vocal performers, such as singers or voice artists. Formal training in singing involves enhanced training in the fine-tuned sensorimotor control required to support both solo and ensemble vocal performance [22], and a body of work has already demonstrated advantages for singers compared with non-singing controls in a range of language and accent imitation tasks [23]. Physiologically, proficient singing requires the efficient control of breathing, the coordination of laryngeal muscles to generate the optimal source signal, and further modulation of that source signal through fine control of vocal tract shape [24]. Thus, it could be predicted that expertise in singing might confer advantages for other vocal tasks requiring specific laryngeal muscle modulations, such as in the exaggeration of body size during speech.

Several studies have reported correlates of laryngeal muscle movements in the human neocortex. These include locations in the dorsal part of the human ventral primary motor cortex [25–27], in addition to a more ventral site that may be evolutionarily common to humans and other primates [28–30]. Research in vocalizing humans has associated activation of dorsal larynx motor cortex (LMC) with three primary dimensions of laryngeal muscle activity: (i) adduction versus abduction of the vocal folds to allow phonation and non-voiced exhalation, respectively; (ii) adjustments in vocal

fold tension leading to changes in the fundamental frequency ( $F_0$ ) of the voice; and (iii) vertical shifts in the position of the larynx to change the length of the vocal tract and thus the resonant properties of the voice through concomitant alterations in the formant frequencies (with functional MRI (fMRI): [25–27,31]; with intracortical recordings/stimulation: [29,30,32]). However, there are outstanding questions about what the neural activation patterns in the speech motor cortex might represent (e.g. acoustic targets of speech or articulator kinematics [33]), and how these are coded during speech planning versus execution.

The primary motor cortex in the precentral gyrus is followed by a parallel somatosensory cortex in the postcentral gyrus, which receives proprioceptive feedback from the muscular periphery, among other sensory information. Neuroimaging studies have shown that the primary somatosensory cortex is engaged by both overt and covert speech production [15] and thus could be implicated in both the planning and execution of laryngeal muscle activity. Evidence from highly trained singers has identified regions of the somatosensory cortex proximal to the dorsal LMC whose local activity [34], resting-state connectivity [35], and structure [36] are associated with singing experience. One interpretation of this finding is that it reflects the heightened control and somatosensory/kinaesthetic awareness of vocal musculature associated with extensive musical training in voice [37]. This interpretation is supported by a study that showed that magnetic stimulation of the right somatosensory cortex improved pitch-matching in non-singers, but only when acoustic masking forced them to rely on somatosensory feedback [38]. Together, these studies suggest the possible existence of an area of the somatosensory cortex that is associated with enhanced laryngeal control for singing. However, this finding has not been underpinned by direct measurements of laryngeal position or kinematics. Furthermore, the work described previously was limited to the neural underpinnings of sung behaviours—it is not known if this neural substrate of expert vocal control for singing would extend to speech, for example, as it applies in speakers' attempts to manipulate the physical body traits implied by the quality of their voices.

In order to address research gaps in knowledge about the neural and physiological bases of vocal modulation, the current study set out to measure vocal modulation behaviour in expert and non-expert vocalists, and to investigate the neural representations of the human larynx for speech in both populations. To do this, we conducted a vocal size and pitch imitation task with both highly trained singers and non-singer control participants. Specifically, we created novel versions of the participants' own speech, in which we manipulated the fundamental frequency ( $F_0$ ) and the formant frequencies to simulate target voices with varying perceived pitch and VTL (figure 1*a*). In order to mimic these voices, participants were required to adjust two dimensions of larynx motor behaviour—vocal fold tension, and larynx height in the vocal tract. To make the task challenging, we measured voice imitation across two different vowels (the front vowel /i:/ and the low back vowel /a:/), and for different combinations of acoustic  $F_0$  and VTL shifts. It was anticipated that the high front tongue position for the vowel /i:/ and the low back tongue position for /a:/ would be differentially constraining for larynx raising and lowering, thus adding demand to the vocal control required to articulate the vowel accurately while imitating the voice targets. Further,



**Figure 1.** (a) Schematic of the voice conditions used in the current study. Yellow dots indicate the acoustic conditions used in the MRI experiment; blue dots indicate additional voice targets imitated in the behavioural practice session. (b) Experimental protocol. Top row: overall ordering of scans, where 'rt' stands for real-time anatomical MRI scans of the vocal tract, 'fMRI' stands for functional MRI scans of brain activation, and T1 represents the whole-brain anatomical scan. Middle row: details of the real-time MRI blocks. Participants heard a word over headphones and after 1.2 s were cued to provide a spoken imitation. Stimuli were presented in miniblocks of four trials per condition; condition order was randomized across the block pair. Bottom row: details of the functional MRI trial types. A rapid-sparse routine was employed, in which listening and imitation events occurred during 1.5 s pauses between echo planar imaging (EPI) volume acquisitions. There were three trial types, cued through the colour of an onscreen fixation cross: (1) Listen and Imitate (blue  $\rightarrow$  green for speech onset), (2) Listen Only (yellow) and (3) Rest (white). The Listen and Imitate trials were used to calculate activation to speech preparation and execution. (c) Example real-time MR images of a Singer performing imitation of the five voice target conditions for 'bead'. Each image shows a frame extracted from the steady state of the vocalic portion of the word, labelled according to the target's displacement from the 'normal' voice in pitch and VTL. The yellow and red lines show the vertical position of the larynx and the horizontal position of the lips as obtained from a semi-automated image segmentation routine implemented in MATLAB [39]. Only the larynx height data were analysed for the current study. (d) Axial whole-brain slices showing the group region-of-interest maps for speech preparation (calculated using a contrast of All listen pre-imitate > Rest including all participants; voxel height threshold  $p < 1 \times 10^{-7}$  family-wise error corrected (FWE), cluster threshold  $p < 0.05$  FWE) and speech execution (calculated with a contrast of All imitate > Rest including all participants; voxel height threshold  $p < 0.05$  FWE, cluster threshold  $p < 0.05$  FWE). RSA, representational similarity analysis. See Methods and electronic supplementary material for further details. (Online version in colour.)

as  $F_0$  and VTL typically covary negatively across human voices (i.e. adult males have longer VTLs and lower pitches than adult females and children), we predicted that including atypical combinations of voice parameters (e.g. short VTL with lowered pitch; long VTL with raised pitch) should also add difficulty to the task. Both design choices were thus made to maximize the discriminability of expert versus non-expert vocal control. In the imitation task, participants produced heard targets after a short delay (1–2 s), such that in an fMRI experiment we could model neural activation separately for speech preparation (i.e. hearing targets and planning speech) and speech execution—this allowed us to inspect representations of imitated voice parameters during different stages of speech production. During the fMRI

runs, acoustic speech imitations were recorded to allow extraction of  $F_0$  as a measure of vocal fold tension, while task-related vertical movements of the larynx were measured during interleaved blocks of real-time anatomical MRI (rtMRI) of the vocal tract (see figure 1b for design). Using multivariate analyses of behaviour and neural activation (representational similarity analysis, RSA; [40]) during speech preparation and execution, we aimed to measure imitation accuracy and locate the representation of pitch/vocal fold tension and VTL/larynx height during the two phases of speech imitation. We predicted that expertise in singing would generalize to greater speech imitation accuracy in the singers, and reveal more robust corresponding neural representations of laryngeal activity in this group.

## 2. Methods

### (a) Participants

A total of 57 adults (20 male; mean age = 24.7 years, s.d. = 5.7, range = 19–43 years) with healthy hearing and no neurological illness (both self-reported) completed the study. Twenty-seven participants (10 male; mean age = 27.5 years, s.d. = 6.4, range = 20–43 years) were highly trained singers, with the primary recruitment criterion that they should have studied/be studying voice performance as the principal instrument in their first university or music college degree. One singer participant did not meet this criterion, but reported extensive singing experience (32 years) and ongoing engagement with singing practice and performance. The remaining 30 participants (10 male; mean age = 22.1 years, s.d. = 3.4, range = 19–35 years) formed a control group. This included one participant who had reported as a singer with 5 years of experience, but did not meet the degree criterion. All participants completed a questionnaire on their music and language experience, which showed that the singers had on average 16.3 years of experience and/or education in voice (range = 5–35 years) and all currently practised singing. Across the sample, participants reported some experience and/or education in voice and musical instruments (Singers: mean = 3.3 instruments, range = 2–6; Controls: mean = 0.8 instruments, range = 0–3) and in languages additional to English (Singers: mean = 1.7 additional languages, range = 0–6; Controls: mean = 1.4 additional languages, range = 0–4). Thus, the main distinction between the participant groups was in their probable level of singing expertise, and we did not control for overall levels of musical or linguistic experience. All participants gave informed consent, and the study was approved by the Ethics Committee at the Department of Psychology, Royal Holloway, University of London.

Seven participants (five Controls, two Singers) were excluded from the fMRI analyses owing to an error with slice positioning; the remaining 50 were used in the calculation of the RSA region-of-interest (ROI) maps. A final sample of 49 participants<sup>1</sup>, comprising 24 Singers (9 male; mean age = 28.1 years, s.d. = 6.5, range = 21–43 years) and 25 Controls (8 male; mean age = 22.1 years, s.d. = 3.7, range = 19–35 years), was used in the statistical analyses of behavioural pitch imitation and in all searchlight analyses of brain activation. Larynx height could not be tracked for two of these participants, owing to MR signal dropout (1 Control) and pervasive errors with the automated labelling of larynx height (1 Singer). Thus, the reported group analyses involving VTL imitation behaviour include a group of 47 participants comprising 23 Singers (9 male; mean age = 28.2 years, s.d. = 6.7, range = 21–43 years) and 24 Controls (8 male; mean age = 22.1 years, s.d. = 3.7, range = 19–35 years). We note that while we achieved good matching of the male-to-female ratio across groups, it was not possible to recruit more males owing to a lack of availability of volunteer participants—we therefore do not report analyses on the effects of participant sex.

### (b) Stimuli

All audio speech data collected during the behavioural session were recorded with a condenser microphone (Røde NT1-A; RØDE Microphones, Silverwater, Australia) and digitized through a PreSonus AudioBox USB recording system (PreSonus Audio Electronics, Baton Rouge, LA). The experimental stimuli comprised 18 versions of the monosyllabic words ‘bead’ and ‘bard’, generated from recordings of the participant’s voice.

Participants produced five instances of ‘bead’ and ‘bard’ in a short carrier phrase (e.g. ‘Say the word: BEAD’), following instructions to produce the words at a normal pitch and with a slightly longer than natural duration (this was in order to obtain a sufficiently long vowel steady-state portion for imitation and acoustic/vocal tract analysis in the main experiment). The

experimenter selected one representative token of each word, aiming for a duration of 0.6–0.8 s and good voice quality (e.g. without vocal fry, which introduces distortions in the synthesis of target stimuli). Tokens were inspected, excised and saved using Praat ([www.fon.hum.uva.nl/praat/](http://www.fon.hum.uva.nl/praat/)).

The two selected tokens (one ‘bead’ and one ‘bard’) were then transformed into acoustically manipulated targets using a modified version of a procedure developed by Chris Darwin at the University of Sussex ([http://www.lifesci.sussex.ac.uk/home/Chris\\_Darwin/Praatscripts/VTchange](http://www.lifesci.sussex.ac.uk/home/Chris_Darwin/Praatscripts/VTchange)) that allows adjustment of the  $F_0$  and speech spectrum as ratios of the original stimulus values. To make clear the distinction between this acoustic modulation and actual VTL, we here refer to the manipulated stimulus parameter as ‘acoustic VTL’ or ‘acVTL’.

A central, ‘normal voice’ version of each word was produced, in which the acVTL was unchanged but the  $F_0$  was shifted two semitones upward from the original (to allow the generation of lower-pitched targets that would not go beyond the speaker’s natural range). In addition, there were eight modified versions of ‘bead’ and ‘bard’, in which the acVTL and  $F_0$  were further adjusted relative to the ‘normal voice’, either by shifting both the  $F_0$  and acVTL by two or four semitones in the same direction (i.e. +2  $F_0$ , +2 acVTL; –4  $F_0$ , –4 acVTL), or in opposite directions (i.e. +2  $F_0$ , –2 acVTL; –4  $F_0$ , +4 acVTL). This process yielded final voice targets with  $F_0$  ranging from 89 to 140% of the participant’s original  $F_0$  in Hz. Assuming a linear relationship between formant frequencies and physical VTL, the apparent VTLs of the voice targets ranged from 79 to 126% of the participant’s actual VTL in centimetres. Figure 1a depicts the two resulting ‘axes’ of voice targets used in the experiment.

The ‘normal voice’ and all eight modified voices were used in a behavioural practice session (see electronic supplementary material for details), while the ‘normal voice’ and the four most extreme modified voices were used in the MRI session. For use in the MRI scanner, stimuli were further filtered with earbud-specific parameters for use with Sensimetrics earbuds (S14; Sensimetrics, Malden, MA), then parametrically equalized (filter CF: 3.5 kHz; 10 dB gain; Q-factor = 2), and normalized (root-mean-square) with Adobe Audition (Adobe, San Jose, CA)—these steps ensured that all stimuli were clearly distinguishable against continuous rtMRI acquisition noise.

### (c) Behavioural practice session

#### (i) Training video

The participant viewed a short presentation (lasting approx. 4 min) in Microsoft PowerPoint (Microsoft, Albuquerque, NM), in which they were introduced to examples of modified stimuli of the type used in the experiment (presented over headphones) and instructed how to perform the imitation task. The presentation can be found in the supporting data for this paper (<https://osf.io/6pqt/>). Additional description of the training can be found in the electronic supplementary material.

#### (ii) Imitation practice

Participants completed a short practice task in which they produced imitations of all 18 voice targets ((1 normal voice + 8 modulated targets) × 2 words). Stimulus presentation and data collection were performed using MATLAB (MathWorks, Natick, MA) with the Psychtoolbox extension [41]—see the electronic supplementary material for further details of the stimulus presentation and recording. Each condition was presented in miniblocks of five trials (two miniblocks per condition) and the order of conditions was pseudorandomized. Participants were given the opportunity for a short break every six miniblocks. Analyses of these data will not be discussed here.

## (d) MRI session

### (i) MRI procedure

All stimuli were delivered through MR-compatible earbuds; speech was recorded with a fibre-optic microphone (FOMRI-III; OptoAcoustics, Or Yehuda, Israel). All stimuli were presented, and speech output recorded, digitized and saved, via the Psychophysics toolbox running in MATLAB, with back projection for the presentation of visual stimuli. For MRI acquisition parameters, please see the electronic supplementary material.

In the scanner, participants listened to and imitated the central (normal) voice condition and the four most extreme voice transformations (i.e. the endpoints of the axes tested in the behavioural practice; figure 1*a*) only. A pair of rtMRI runs (63 s each) was presented before each of the three fMRI runs (approx. 13 min each), and the session ended with a T1-weighted whole-brain structural scan. The total duration of the scans was around 1 h (figure 1*b*).

fMRI data were acquired using a rapid-sparse, event-related protocol, with auditory stimuli and speech production events timed to occur during short silent periods between the acquisition of whole-brain volumes. Each Listen and Imitate trial occurred over two dynamic acquisitions (i.e. 2 periods of acquisition + delay). Participants listened to a particular voice target condition, and imitated it when cued after the next acquisition. This enabled us to separately capture blood oxygen level dependent (BOLD) activation reflecting speech preparation and the subsequent execution of the speech. Listen Only and Rest trials occurred in a single dynamic acquisition (figure 1*b*). Similarly to our previous work [42,43], we distinguish speech preparation from passive listening using the event labels 'listen pre-imitate' and 'listen only', respectively. Three trial types were thus presented during fMRI: Listen and Imitate (comprising listen pre-imitate and imitation events), Listen Only, and Rest. Results of Listen Only trials are not discussed here.

The structure of fMRI trials is illustrated in figure 1*b*. Four miniblocks of 35 trials (20 Listen and Imitate (2 per speech target), 10 Listen Only (1 per speech target) and 5 Rest) were presented per fMRI run, for a total of 140 trials. The trial order was randomized separately within each miniblock. Each fMRI run lasted approximately 13 min. Before entering the scanner, participants completed a practice fMRI miniblock of 35 trials (no speech data were recorded during this practice).

rtMRI blocks comprised pairs of 63 s runs. Across a pair of runs, participants imitated all 10 voice targets. Each target condition (e.g. 'normal bead') was delivered in a miniblock of four consecutive trials, for a total of 20 trials per run. The order of miniblocks was randomized across the two runs. Each trial began with the delivery of an audio stimulus and a visual prompt (Listen), followed after 1.2 s by a prompt to imitate (Repeat) and a 1.5 s gap in which the participant produced their imitation.

## (e) Data processing

### (i) Acoustic data

All participant imitations from the fMRI runs were subjected to an acoustic analysis in Praat to extract trialwise mean fundamental frequency ( $F_0$ ) in Hz from the vocalic portion of each utterance. Stimuli were analysed in batch per condition, with trial-by-trial visual inspection of the  $F_0$  and adjustment of the measurement parameters if necessary (see electronic supplementary material for exclusion criteria). We calculated the mean condition-wise  $F_0$  shifts separately for 'bead' and 'bard' by subtraction from the mean  $F_0$  for the 'normal' voice condition, such that performance was expressed in terms of the shift of  $F_0$  in semitones relative to the central voice target in figure 1*a*.

## (ii) Vocal tract MRI data

Vocal tract MRI images were compiled into one AVI file per run pair. From each video, images were cropped to  $68 \times 68$  pixels covering the whole vocal tract area. Larynx coordinates were identified and extracted frame-by-frame using a custom MATLAB toolbox [39]; larynx  $y$ -coordinates (in pixels) were averaged across the steady-state portion of the vowel in each imitated word, then across all trials for that condition (see electronic supplementary material for exclusion criteria). Separately for 'bead' and 'bard', the mean coordinate for each modulated condition was normalized relative to the mean of the 'normal' voice tokens for that run, then averaged across the three runs. These values were used in the construction of vocal tract-derived dissimilarity matrices of larynx height for RSA analyses (see below). Figure 1*c* illustrates example frames from the output of the larynx-tracking analysis from one Singer.

## (iii) Functional MRI analysis

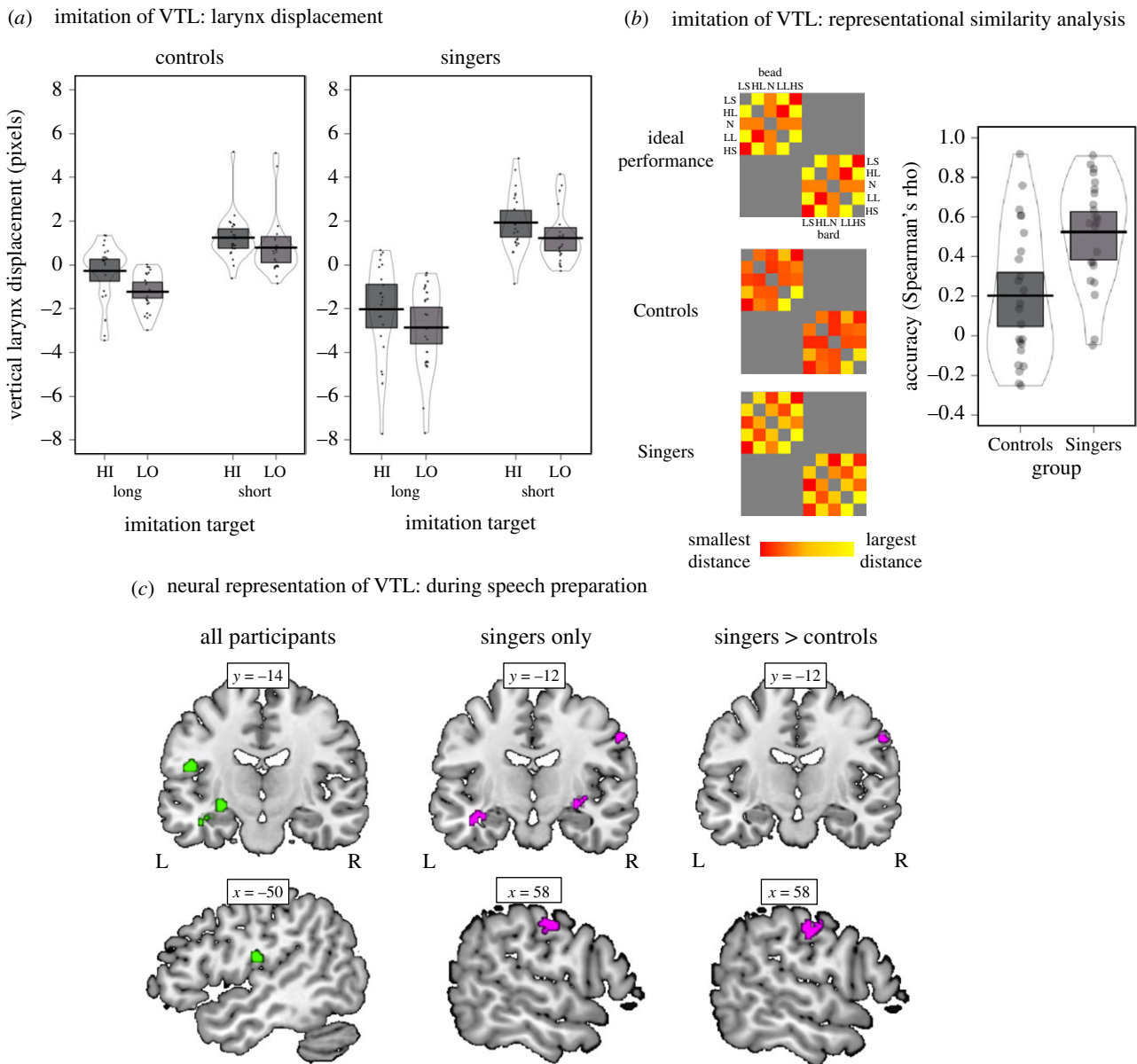
fMRI images were preprocessed within MATLAB using the SPM12 toolbox (<https://www.fil.ion.ucl.ac.uk/spm/>). Per subject, raw echo planar imaging (EPI) images were realigned, coregistered to the anatomical image, normalized to Montreal Neurological Institute (MNI) space (and resampled to 2 mm isotropic), and smoothed with a Gaussian kernel of 8 mm full width at half maximum (FWHM). Data were then analysed in a first-level general linear model, in which listen only, listen pre-imitate, and imitate events were modelled as regressors—separately for each 'bead' and 'bard' target—and convolved with the canonical haemodynamic response function in SPM. Listen only and listen pre-imitate events were modelled at the onset of the auditory stimulus. Imitate events were modelled as coincident with the appearance of cue to speak (a green cross; figure 1*b*). Six motion parameters (describing translations and rotations about the  $x$ ,  $y$  and  $z$  axes) were included as regressors of no interest. For each subject,  $T$ -contrasts were calculated for (1) All listen pre-imitate events > Rest (conditions collapsed), (2) All imitate events > Rest (conditions collapsed), (3–12) Each listen pre-imitate (speech preparation) condition > Rest (i.e. separate contrasts for each 'bead' and 'bard' target) and (13–22) Each imitate condition > Rest.

## (f) Statistical analysis

### (i) Behavioural data

*Analysis of larynx displacement and  $F_0$  shifts.* Behavioural data were analysed using linear mixed-effects models within the *lme4* [44] package in the R environment. Outcome variables were (i) mean vertical larynx displacement (pixels) and (ii) mean  $F_0$  shift. Fixed factors were Group (Singers, Controls), VTL (long, short), Pitch (high, low) and Word (bead, bard). Participants were modelled as random intercepts. Significance of interactions and main effects was established via likelihood ratio tests, in which a model containing the effect of interest was contrasted with a reduced model lacking the effect. For both outcome measures, the full linear model including the effect of Word produced a singular fit; therefore this factor was removed. For  $F_0$  shifts, removing the main effect of Pitch generated a singular fit, so for this main effect we instead report the coefficient statistic and its associated significance, obtained using the *sjPlot* [45] package in the R environment.

*Representational similarity analysis.* In order to model performance on the behavioural task, we constructed two  $10 \times 10$  representational dissimilarity matrices (RDMs) for each participant. Cells within these matrices described the absolute pairwise distances between the different 'bead' and 'bard' targets in (i)  $F_0$  (semitones) and (ii) Larynx height (pixels). For each participant, these matrices were then compared with two ideal  $10 \times 10$



**Figure 2.** Imitation and neural representation of vocal tract length (VTL). (a) Vertical larynx movement during the imitation of modulated speech targets. Data are plotted as the mean upward/downward larynx height excursion from the normal voice, where downward movements are negative. Results are shown collapsed across both word contexts (bead, bard). HI, higher-pitched targets; LO, lower-pitched targets; long, longer VTL targets; short, shorter VTL targets. Plots were created using the *pirateplot* function within the *yarr* package in R [47]. Bold horizontal lines show the means per group and condition, boxes indicate 95% Bayesian highest density intervals, dots indicate data from individual participants. (b) Behavioural representational similarity analysis (RSA) for the imitation of VTL. Measures of vertical larynx displacement in pixels (relative to the ‘normal voice’) were used to generate representational dissimilarity matrices (RDMs) for each participant, which were compared with an ideal model (based on the inter-stimulus VTL distances in semitones) using Spearman’s correlation tests. The figure shows the ideal model (LS, low  $F_0$ , short VTL; HL, high  $F_0$ , long VTL; N, normal voice; LL, low  $F_0$ , long VTL; HS, high  $F_0$ , short VTL) as well as the corresponding mean group RDMs for the Singers and Controls and a plot of accuracy by group (created using the *pirateplot* function within the *yarr* package in R [47]). Bold horizontal lines show the means per group, boxes indicate 95% Bayesian highest density intervals, dots indicate data from individual participants. (c) Results of neural RSA searchlight analyses conducted within the CoSMoMVPA toolbox [46] implemented in MATLAB. Areas of activation indicate regions showing a significant correlation between neural activation patterns during speech preparation and the ideal performance model for VTL imitation. Group images are shown at a voxel height threshold of  $p < 0.001$  and a corrected cluster threshold of  $p < 0.05$  FWE. Coordinates are in Montreal Neurological Institute stereotactic space. (Online version in colour.)

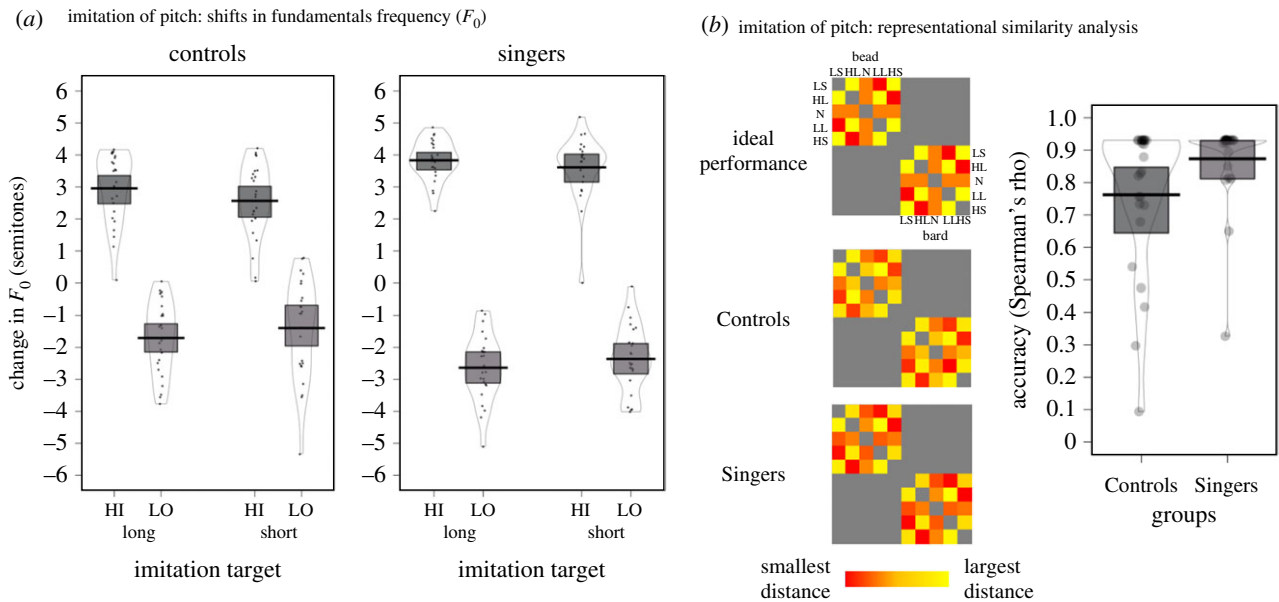
model RDMs describing the underlying relationships between target stimuli in pitch (semitones) and VTL (semitones), using Spearman correlation tests within the CoSMoMVPA toolbox [46] implemented in MATLAB. Figures 2b and 3b depict the model matrices alongside the group-averaged performance matrices for Singers and Controls.

Group analyses of these Spearman correlation scores were conducted in the R environment: Mann–Whitney tests within the *coin* package [48] were used to compare performance between the two groups, and one-sample Wilcoxon tests to compare performance against zero. Finally, Spearman correlation was

used to test the significance of the relationship between performance and years of experience in voice, separately for pitch and VTL, in Singers only.

### (ii) Functional MRI data

*Representational similarity analysis.* RSA on functional neuroimaging data was carried out using the searchlight function within the CoSMoMVPA toolbox. Two candidate RDMs—the ideal pitch model and the ideal VTL model—were used to searchlight neural activation separately for (i) the listen pre-imitate (speech



**Figure 3.** Imitation of pitch. (a) Changes in  $F_0$  during the imitation of modulated speech targets. Data are plotted as the mean upward/downward pitch excursion from the normal voice, where downward changes are negative. Results are shown collapsed across both word contexts (bead, bard). HI, higher-pitched targets; LO, lower-pitched targets; long, longer VTL targets; short, shorter VTL targets. RDI plots were created using the `pirateplot` function within the `yarr` package in R [47]. Bold horizontal lines show the means per group and condition, boxes indicate 95% Bayesian highest density intervals, dots indicate data from individual participants. (b) Behavioural representational similarity analysis (RSA) for the imitation of pitch. Measures of  $F_0$  change in semitones (relative to the 'normal voice') were used to generate representational dissimilarity matrices (RDMs) for each participant, which were compared with an ideal pitch model (based on the inter-stimulus  $F_0$  distances in semitones) using Spearman's correlation tests. The figure shows the ideal model (LS, low  $F_0$ , short VTL; HL, high  $F_0$ , long VTL; N, normal voice; LL, low  $F_0$ , long VTL; HS, high  $F_0$ , short VTL) as well as the corresponding mean group RDMs for the Singers and Controls and a plot of accuracy by group (created using the `pirateplot` function within the `yarr` package in R [47]). Bold horizontal lines show the means per group, boxes indicate 95% Bayesian highest density intervals, dots indicate data from individual participants. (Online version in colour.)

preparation) phase and (ii) the imitate (speech execution) phase of speech imitation trials. The neural data were RDMs generated from smoothed  $T$ -maps of the single-subject contrasts of each condition > Rest. To constrain the searchlight analyses to regions showing significant activation associated with speech preparation and speech execution, respectively, we used group masks of (i) All Listen Pre-imitate > Rest for the listen pre-imitate data and (ii) All imitate > Rest for the imitate data. The group regions of interest ROIs were generated using second-level one-sample  $T$ -tests on all participants, calculated in SPM. In order to ensure that each mask was of comparable volume, the Listen Pre-imitate (i.e. speech preparation) mask was created at a voxel height threshold of  $p < 1 \times 10^{-7}$  family-wise error corrected (FWE) and a corrected cluster threshold of  $p < 0.005$  FWE (yielding 18 128 voxels), while the imitation (i.e. speech execution) mask had a more liberal voxel height threshold of  $p < 0.005$  FWE and a corrected cluster threshold of  $p < 0.05$  FWE (yielding 10 897 voxels; see figure 1d). The searchlight process involved extracting  $10 \times 10$  RDMs describing the distances (as Spearman correlation coefficients) between activation (Listen Pre-imitate or Imitate) in spherical searchlight volumes (radius: 4 mm) centred around each voxel in the ROI. Spearman correlation tests were applied iteratively to compare these neural RDMs with the relevant candidate RDM (i.e. ideal pitch model or ideal VTL model) across the brain—the resulting correlation coefficients were Fisher  $z$ -transformed before being converted back to Pearson correlations for use in the group analyses. Each searchlight analysis thus generated a map of correlation coefficients per subject.

Group analyses of the searchlight maps were carried out using nonparametric permutation-based tests implemented in the `SnPM` toolbox (v. 13.1.06; <http://warwick.ac.uk/snpm>). For within-group comparisons of coefficients with zero we used the 'one-sample  $T$ -test' module: this test was applied separately for each searchlight analysis on (i) Singers only, (ii) Controls

only and (iii) all participants. For comparisons of the searchlight maps between Singers and Controls, we used the 'two-sample  $T$ -test'. For an exploratory analysis of the effects of experience on representations of VTL in Singers only, we used the 'simple regression' module. For all analyses, we applied 10 000 permutations and no variance smoothing.

### 3. Results

#### (a) Imitation of vocal tract length

During imitation, Singers displaced their larynx on average by 1.6 pixels/4 mm upward (s.d. = 1.3 pixels/3.3 mm; range = 0.9 pixels/2.3 mm downward to 4.9 pixels/12.3 mm upward) and 2.4 pixels/6 mm downward (s.d. = 2.1 pixels/5.3 mm; range = 7.7 pixels/19.3 mm downward to 0.7 pixels/1.8 mm upward) relative to the normal voice to imitate modulated targets with short and long VTLs, respectively. This compared with an average of 0.7 pixels/1.8 mm upward (s.d. = 1.2 pixels; range = 0.8 pixels/2 mm downward to 5.2 pixels/13 mm upward) and 1.0 pixels/2.5 mm downward (s.d. = 1.3 pixels; range = 3.4 pixels/8.5 mm downward to 1.3 pixels/3.3 mm upward) for Controls.

Analysis using linear mixed models identified a significant two-way interaction of Group  $\times$  Length ( $\chi^2_1 = 42.36$ ,  $p < 0.001$ ), and main effects of Group ( $\chi^2_1 = 70.06$ ,  $p = 0.008$ ), Length ( $\chi^2_1 = 187.54$ ,  $p < 0.001$ ) and Pitch ( $\chi^2_1 = 18.63$ ,  $p < 0.001$ ). Figure 2a illustrates these results: Singers made more pronounced vertical displacements for both the long VTL and short VTL targets compared with controls, while both groups showed a lower vertical larynx position when imitating longer vocal tracts and lower-pitched targets.

RSA was used to compare vertical larynx movements in each participant with a model describing ideal performance on VTL imitation. This identified significant correlations with the model in Singers (median Spearman's rho: 0.569,  $z = 40.09$ ,  $p < 0.001$ ), and in Controls (although this relationship was weaker; median Spearman's rho: 0.149,  $z = 2.24$ ,  $p = 0.012$ ). A direct comparison of the two groups confirmed a significantly better fit to the model for Singers than Controls ( $z = 2.99$ ,  $p = 0.003$ ; see figure 2*b*). However, a further Spearman correlation analysis revealed no significant relationship between Singers' RSA scores and the number of years of experience in voice.

RSA searchlight analyses of neural activation supported these findings (figure 2*c*; electronic supplementary material, table S1), with a stronger representation of the ideal VTL model for Singers (versus Controls) during speech preparation in right pre-/post-central gyrus (with the peak in somatosensory area S1). Taken alone, the Singers showed significant representation of VTL during speech preparation in an overlapping region of the right central sulcus/post-central gyrus, and in additional volumes within the hippocampus and thalamus. However, there was no significant correlation between the strength of neural representations and the number of years of experience in voice. An analysis of all participants revealed significant representation of VTL in the left ventral post-central gyrus during speech preparation. There was no evidence of significant representations in the Control group alone at the chosen threshold.

### (b) Imitation of pitch

During imitation, Singers shifted voice  $F_0$  on average by 3.7 semitones up (s.d. = 0.8; range: 0 up to 5.2 up) and 2.5 semitones down (s.d. = 10.0; range: 5.1 down to 0.1 down) relative to the normal voice for high- and low-pitched targets. This compared with an average of 2.8 semitones up (s.d. = 1.1; range: 0.1 up to 4.2 up) and 1.6 semitones down (s.d. = 1.3; range: 5.3 down to 0.8 up) for controls (figure 3*a*).

Analysis using linear mixed models identified significant two-way interactions of Group  $\times$  Pitch ( $\chi^2_1 = 69.13$ ,  $p < 0.001$ ) and Pitch  $\times$  Length ( $\chi^2_1 = 7.75$ ,  $p = 0.005$ ) and a significant main effect of Pitch ( $t = -43.24$ ,  $p < 0.001$ ). The effects can be observed in figure 3*a*. All participants distinguished between high- and low-pitched targets through shifts in the  $F_0$  of their imitations. Within this, Singers tended to make more pronounced upward and downward shifts in  $F_0$  than Controls, while both groups showed relatively smaller excursions in  $F_0$  for short VTL targets compared with long VTL targets.

RSA of the  $F_0$  of the spoken imitations showed that both the Singers and Controls performed well (figure 3*b*), with median Spearman's correlation coefficients between each participant's performance and the ideal pitch model well above chance for both Singers (median Spearman's rho: 0.931,  $z = 4.40$ ,  $p < 0.001$ ) and Controls (median Spearman's rho: 0.834,  $z = 4.38$ ,  $p < 0.001$ ). When directly compared, there was a significant difference between the groups ( $z = 2.18$ ,  $p = 0.03$ ), indicating that trained Singers performed better than non-singing Controls at adjusting  $F_0$  upward and downward to match the voice targets. However, a Spearman correlation analysis revealed no significant relationship between Singers' RSA scores and the number of years of experience in voice.

Despite the behavioural advantage for Singers, our searchlight analyses of neural activation data found no difference between groups in the neural representation of the ideal pitch model during speech preparation or speech execution. Further, we found no significant evidence for the representation of the ideal pitch model during speech preparation or speech execution in either group separately, or in the combined participant group.

## 4. Discussion

We measured imitation of voice pitch and VTL in adult singers and non-singers, and probed the neural representations of laryngeal muscles during preparation and execution of imitations. Each participant imitated speech targets that were selectively manipulated relative to their normal voice. By using acoustic measures of  $F_0$  alongside larynx position metrics from vocal tract MRI images, we could directly and precisely measure the contributions of intrinsic (vocal fold) versus extrinsic larynx musculature to speech imitations. Furthermore, by comparing performance in trained singers and a group of non-singer control participants, we harnessed differences in vocal expertise to reveal the underlying neural representations of VTL for speech imitation.

We showed that both singers and controls can volitionally modulate vocal parameters in a goal-directed fashion to imitate voices of different sizes and pitches, in line with previous work investigating volitional vocal size exaggeration [16,17]. Specifically, we showed that both groups adjusted  $F_0$  downward and upward to imitate lower- and higher-pitched voice targets, respectively and, for the first time, we also showed that modulations to imitate longer and shorter VTLs were achieved via appropriate upward and downward movements of the larynx in the vocal tract. As predicted, singers showed larger modulations of both parameters, which in both cases were more closely correlated with an ideal model of imitation behaviour. Thus, we replicate previous findings that expertise in singing generalizes to enhanced performance on speech tasks [23], here for two parameters of laryngeal sensorimotor control.

Using multivariate searchlight analysis of neural activation data, we identified representation of VTL in both cortical and subcortical sites during preparation to speak. A region of the left somatomotor cortex identified in the whole participant group did not correspond topographically to previous reports of the LMC. However, a further direct comparison of singers and controls revealed an expertise-related enhancement of VTL representation in the right somatosensory cortex, just posterior to the reported location of the dorsal LMC in humans [16–18]. We speculate that this site could represent a larynx sensory cortex that is closely coupled to its corresponding LMC during speech motor control [9]: in line with this, probabilistic diffusion tractography analyses of LMC connectivity have revealed dramatically stronger connectivity with somatosensory and inferior parietal cortices in humans than in macaques [49]. However, we also note that although the pre-central gyrus is predominately associated with motor-related activity and the post-central gyrus with somatosensation, recent neuroimaging and neurostimulation data suggest that these functional divisions do not always align with gross anatomical landmarks [32,50]. Hence, we refrain from claiming the precise nature of the representations here as somatosensory.



To date, only one study has explicitly investigated the neural correlates of extrinsic laryngeal muscle activity, using univariate analysis of BOLD fMRI data. Belyk & Brown [31] scanned (non-expert) participants while they displaced the larynx in a downward direction, or in both downward and upward directions, and compared the spatial distribution of activation with that measured during phonation (i.e. vibration of the vocal folds). When participants were asked to move the larynx vertically, without speaking, the investigators observed extensive activation covering the ventrolateral sensorimotor cortex in both hemispheres, which included the dorsal LMC. Our results extend this finding, as we show that the post-central gyrus houses representations of VTL during speech that are associated with expertise-related group differences in voice modulation through larynx movement.

Previous work on imagined speech and song suggests that imagery can engage similar neural responses to overt execution of spoken and sung vocal behaviour [15,37]. Our findings of representation of VTL during preparation to speak echo those of our previous study on vowel imitation, in which we reported robust evidence for the neural representation of articulatory information (using both vocal tract MR images and acoustic models of formant characteristics) prior to speech execution [42]. In that study, we showed that the raw acoustic properties of the target vowel stimuli were insufficient to account for our findings, suggesting that the identified regions thus contained information related to articulation rather than acoustics *per se*. In the current study, we demonstrate that representation of VTL during speech preparation was stronger in trained singers, who could more effectively imitate VTL through the vertical displacement of the larynx. We argue that the regions implicated here may be critically involved in the conversion of auditory input to motor output [51], although we cannot rule out the contribution of actual larynx movement during this phase. Also in line with our previous study, we found no evidence for the representation of VTL during activation related to speech execution. The current paradigm was sufficient to obtain robust activation during imitation (figure 1*d*)—nevertheless, as we previously described [42], there may be specific considerations for probing the properties of overt speech behaviour that are not well suited to the current method of investigation. For example, owing to the somatotopic arrangement of the motor cortex, it may be that the overall activation of laryngeal motor regions during phonation is sufficiently high to obscure relational differences associated with  $F_0$  or larynx height. These may, therefore, be better captured before speech onset.

Despite robust representation of the pitch model in the imitative behaviour of both singers and controls, we found no evidence of pitch representation in neural activation patterns. We deliberately constrained pitch targets to be within a comfortable range of  $\pm 4$  semitones. By contrast, the eight-semitone range in VTL in the current study was quite extreme: changes in VTL sufficient to yield a percept of a change in talker identity are around half as large as for  $F_0$  (pitch), suggesting that talkers typically vary VTL much less than  $F_0$  in everyday speech [52]. Indeed, even when participants are asked to exaggerate body size volitionally during speech, they tend to make more substantial changes in  $F_0$  than VTL [16]. The extent of the  $F_0$  shifts chosen for our task, in terms of their perceptual salience and/or the physiological demand of imitating them, may, therefore, have been

insufficient to detect pitch representations in the neural data, in comparison with the more exaggerated VTL targets. However, a recent study with choral singers explored responses to four levels of sung pitch spanning a much wider range (21 semitones), and found no evidence for representation (using a searchlight with a four-way multivariate classifier; [53]). An alternative possibility is that the larynx's intrinsic musculature may be represented neurally in a more fine-grained way linked to ongoing prosodic modulation rather than mean pitch. This argument is supported by recent work using electrocorticography in pre-surgical patients, in which the intonation contour of spoken sentences and sung phrases was tracked by the high gamma activity of electrodes located in dorsal LMC [21].

Several previous studies have explored the neural correlates of vocal expertise, revealing effects on regional activation and structure, as well as connectivity [34–36,53–55]. In the current study, we found a significant difference between singers and non-singer controls in the spoken imitation of VTL, and in the neural representation of this vocal parameter. The neural locus of stronger VTL representations in singers has been previously linked to singing experience [34–36] and proposed as a correlate of enhanced larynx control and kinaesthetic awareness in singing [37]—our MRI data on larynx position and neural representations corroborate this claim, and extend it to the imitation of speech. There is substantial overlap between the neural systems engaged during speech and song production [56], and the components of vocal imitation tested here—perceiving an auditory target, converting it to a motor plan, activating that plan and monitoring and compensating for sensory feedback errors—are likely to share commonalities across these domains. But it remains unclear whether the expertise-related activations reported here indeed reflect singers' enhanced sensorimotor processing within a common vocal control system for speech and song, or if they arise because singers were using a singing strategy to perform our speech imitation task. Using a wider range of spoken and sung tasks in future work will help to delineate this further.

Our analyses suggested that performance on our vocal imitation task was not related to the number of years of singing experience. However, our sampling strategy was not appropriate to investigate the effects of the frequency and recency of singing practice, which might have impacted this result [34]. We also did not control for broader musical experience across our sample of singers and controls. Thus, the observed group differences in our study could be the result of specific training in voice, general musical training ([57]; though see [23]), the level of ongoing singing practice [34], aspects of innate pre-disposition toward vocal/musical activities [58], or some combination of these. Investigation of a variety of expert groups (e.g. instrumentalists, voice artists) can resolve these factors to better understand the specific contributions of singing expertise to vocal imitation. Further, future studies with non-singing controls should explore the extent to which task-specific training on speech imitation (e.g. with real-time vocal tract feedback of larynx position) can enhance the performance of vocal imitation and its neural representation.

## 5. Conclusion

We have provided a novel representational account of laryngeal control in the human cerebral cortex by combining

speech acoustics with MRI of the brain and vocal tract. We have demonstrated generalization of singing expertise to enhanced performance in a vocal size and pitch imitation task, and identified a possible common neural substrate in the somatosensory cortex.

**Data accessibility.** Supporting data are available on the Open Science Framework (<https://osf.io/6pqqk/>).

**Authors' contributions.** C.M. designed the study. S.W., E.K., N.L., M.B., C.L. and C.M. collected and/or analysed data. D.C., M.M. and V.C. developed bespoke tools for data collection and analysis. All authors contributed to the writing and approval of the manuscript.

**Competing interests.** We declare we have no competing interests.

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